

Insulin resistance predicts brain amyloid deposition in late middle-aged adults

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Abstract

Background: Insulin resistance (IR) increases Alzheimer's disease (AD) risk. IR is related to greater amyloid burden post-mortem and increased deposition within areas affected by early AD. No studies have examined if IR is associated with an in vivo index of amyloid in the human brain in late middle-aged participants at risk for AD.

Methods: Asymptomatic, late middle-aged adults (N = 186) from the Wisconsin Registry for Alzheimer's Prevention underwent [C-11]Pittsburgh compound B (PiB) positron emission tomography. The cross-sectional design tested the interaction between insulin resistance and glycemic status on PiB distribution volume ratio in three regions of interest (frontal, parietal, and temporal).

Results: In participants with normoglycemia but not hyperglycemia, higher insulin resistance corresponded to higher PiB uptake in frontal and temporal areas, reflecting increased amyloid deposition.

Conclusions: This is the first human study to demonstrate that insulin resistance may contribute to amyloid deposition in brain regions affected by AD.

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Keywords:

Insulin resistance; Amyloid; PiB; Alzheimer's disease; Cognitively normal; Prefrontal

1. Background

The etiopathogenesis of Alzheimer's disease (AD) is partly characterized by extracellular β -amyloid (A β) aggregation and medial temporal lobe atrophy [1]. Insulin resistance (IR) is associated with brain amyloidosis in rodents and humans [2–6]. IR is characterized by the loss of tissue

responsivity to insulin and progressive compensatory peripheral hyperglycemia. Some studies suggest that higher IR is present in AD [1], increases AD risk [7], and is associated with post-mortem A β plaques [8]. IR may increase A β oligomerization and potentiate brain atrophy via neuroinflammation or other downstream effects [9]. Intranasal insulin therapy has been found to conversely increase plasma A β 40/42 ratios and improve cognition [10].

No study has examined the direct association between IR and an in vivo marker of amyloid load in AD-sensitive brain areas in late middle-aged participants. Regions of interest (ROIs) include inferior and medial temporal lobe, ventral prefrontal cortex, and posteromedial cortex [6]. Insulin resistance

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and type 2 diabetes involve multiple mechanistic pathways, and the effect of IR on neural health may differ depending on whether or not hyperglycemia is present [7,11,12].

In this study, we examined if IR was associated with amyloid binding in three AD-sensitive ROIs based on glycemic status, as found in our previous study on IR and glucose uptake [13]. We hypothesized that higher IR, indexed by the homeostatic model assessment of insulin resistance (HOMA-IR) [14], would predict greater amyloid burden using [C-11] Pittsburgh compound B (PiB) [15] positron emission tomography (PET). On an exploratory basis, we also investigated subregions of these areas to provide greater spatial specificity.

2. Methods

2.1. Participants

One hundred and eighty-six late middle-aged adults from the Wisconsin Registry for Alzheimer's Prevention (WRAP) underwent PiB-PET scanning. Demographics are shown in Table 1. Details about selection criteria, recruitment sources, and other aspects are directly discussed elsewhere [16]. Briefly, this ongoing study examines genetic and biological

factors that contribute to the development of dementia-related cognitive decline and neural dysfunction. Participants were classified as either having a positive (FH+) or a negative family history (FH-) of AD. FH+ was defined as having one or both parents with autopsy-confirmed or probable AD as defined by research criteria [17], based on review of medical records and autopsy reports when available. FH- was defined as no formal diagnosis of AD or other significant cognitive decline in either parent, based on information provided by telephone interviews with participants. The inclusion criteria for this study consisted of: normal cognitive function determined by neuropsychological evaluation and consensus meeting similar to Neurological and Communicative Disorders and Stroke-Alzheimer's Disease and Related Disorders Association (NINCDS-ADRDA) recommendations [17], no contraindication for PET or magnetic resonance imaging (MRI) and a subsequently normal MRI scan, no current diagnosis of major psychiatric disease or other major medical conditions (e.g., myocardial infarction, recent history of cancer), and no history of head trauma. The University of Wisconsin Institutional Review Board approved all procedures related to this study. Each participant gave full informed consent before study participation.

2.2. Neuropsychological testing

To confirm that participants in this sample were cognitively normal, the Mini-Mental State Examination (MMSE) and neuropsychological factor scores from the full battery [16] were used (see Table 1). Four cognitive domain factors were derived as described previously [18]: immediate memory, verbal learning and memory, working memory, and speed and flexibility. The individual tests which loaded onto the factors were as follows: (1) Rey Auditory Verbal Learning Test [19], Trials 1 and 2 loaded onto Immediate Memory; (2) Rey Auditory Verbal Learning Test [19], Trials 3 to 5 and Delayed Recall Trial loaded onto Verbal Learning & Memory; (3) Wechsler Adult Intelligence Scale – 3rd edition [20], Digit Span, Arithmetic, and Letter-Numbering Sequencing subtests loaded onto Working Memory; and (4) the interference trial from the Stroop Test [21], and Trail Making Test A and B [22] loaded onto Speed & Flexibility. For the MMSE, a cutoff score of 26 was used based on recommended thresholds from the Alzheimer's Disease Neuroimaging Initiative [23]. It is emphasized here that consensus committee meetings in line with NINCDS-ADRDA recommendations [17] were used to confirm if participants were cognitively normal, rather than just the MMSE and other neuropsychological tests.

2.3. APOE genotype

Apolipoprotein (APOE) genotyping has been described previously [24]. Participants were categorized as “Non-APOE $\epsilon 4$ ” (no $\epsilon 4$ alleles) or “APOE $\epsilon 4$ ” (at least one $\epsilon 4$ allele).

Table 1

Participant demographics

N	186
Age in y (mean \pm SD)	60.37 \pm 5.63
Gender	
Female	129 (69.4%)
Male	57 (30.6%)
Education (mean \pm SD)	16.61 \pm 2.94
Family history of AD	
Negative	53 (28.5%)
Positive	133 (71.5%)
APOE $\epsilon 4$ status	
Non-APOE $\epsilon 4$	114 (61.3%)
APOE $\epsilon 4$	72 (38.7%)
Diabetes status	
Normoglycemia (<100 mg/dl)	135 (72.6%)
At risk/prediabetes (100–125 mg/dl)	43 (23.1%)
Type 2 diabetes (>125 mg/dl)	8 (4.3%)
DBP	74.11 \pm 8.98
SBP	124.70 \pm 15.19
BMI (mean \pm SD)	28.20 \pm 5.22
Glucose (mg/dl)	95.01 \pm 10.28
Insulin (μ U/ml)	9.53 \pm 7.60
HOMA-IR (mean \pm SD)	2.33 \pm 2.19
Total cholesterol (mg/dl)	202.39 \pm 34.79
MMSE (mean \pm SD)	29.3 \pm 0.96
Speed and flexibility (mean \pm SD)	0.13 \pm 0.86
Working memory (mean \pm SD)	0.20 \pm 1.11
Verbal learning (mean \pm SD)	0.16 \pm 0.95
Immediate memory (mean \pm SD)	0.15 \pm 1.07

Abbreviations: SD, standard deviation; AD, Alzheimer's disease; APOE $\epsilon 4$, apolipoprotein $\epsilon 4$ allele; BMI, body mass index; DBP, diastolic blood pressure; SBP, systolic blood pressure; HOMA-IR, homeostatic model assessment of insulin resistance; MMSE, Mini-Mental State Examination.

NOTE. The four cognitive factors at the bottom of Table 1 are Z-scores. Number of subjects is listed unless otherwise specified in parentheses.

2.4. HOMA-IR, body mass index, glycemic status, and other factors

Participants were fasted for 12 h before blood collection. Basal glucose and insulin were measured in serum. As described previously [11], insulin was quantified by standard enzyme-linked immunosorbent assay (R&D Systems, Minneapolis, MN). Homeostatic model assessment of insulin resistance (HOMA-IR) was calculated by taking the product of basal glucose (mg/dl) and basal insulin (μ U/ml) and dividing by 405 [14]. HOMA-IR was treated as a continuous variable for analyses. Body mass index (BMI) was calculated by dividing the participant's weight in kilograms by the square of their height in meters. Hyperglycemia was defined as either (1) having type 2 diabetes or being at risk for type 2 diabetes (i.e., prediabetes) based on American Diabetes Association criteria (i.e., fasting blood glucose levels of 100 mg/dl or greater) or (2) taking medication to control type 2 diabetes. Finally, as described previously [16], diastolic and systolic blood pressure (DBP, SBP) and total cholesterol were acquired.

2.5. MRI: Anatomical

A 3D fast spoiled gradient-echo T1-weighted image was acquired using a 3T General Electric (Waukesha, WI) scanner. Sequence parameters were: TR = 8.1 ms; TE = 3.2 ms; TI = 450 ms; flip angle = 12° ; 256×256 matrix; field of view = 260 mm; slice thickness = 1.0 mm. Images were inspected for artifact or abnormalities that would exclude them from use in PET analyses. No scans were excluded.

2.6. ROIs: FreeSurfer segmentation and parcellation

Our analysis focused on broad ROIs to limit the number of statistical comparisons made. To derive the ROIs, T1-images were preprocessed using FreeSurfer 5.1 software (<http://surfer.nmr.mgh.harvard.edu/>). This software package corrects images for intensity bias, removes the skull, and then uses a probabilistic atlas to segment gray and white matter and classify different subcortical structures, and parcellate and label cortical regions [25]. The 2009 Destrieux atlas was used, which delineates between sulci and gyri before regional classification and offers a more precise method for interpolating surface topology relative to other FreeSurfer atlases. As depicted in Fig. 1, we created three broad ROIs that encompassed ventral frontal, inferior and medial temporal, or posterior parietal regions. Supplementary Fig. 1 depicts the 17 FreeSurfer ROIs ("sub-ROIs") used to construct the three broad ROIs.

2.7. PET: [C-11]PiB synthesis, scanning, and distribution volume ratio maps

Details regarding [C-11]PiB radiochemical synthesis and scanning have been described previously [18]. Briefly, [C-11]PiB was synthesized using a captive solvent method

[26]. Typical yields of final [C-11]PiB product were in excess of 2 GBq, with specific activities of 150–600 GBq/ μ mol. [C-11]PiB PET data were acquired in 3D mode. A 6-min transmission scan was acquired for attenuation correction. A 70-min dynamic [C-11]PiB PET acquisition was then initiated with the injection of a 550 MBq [C-11]PiB bolus, injected over 30 s. Seventeen dynamic acquisition frames were collected. The PET data were reconstructed using a filtered back-projection algorithm with sinogram trimming to a voxel size of $2.57 \text{ mm} \times 2.57 \text{ mm} \times 2.43 \text{ mm}$ and matrix dimension of $128 \times 128 \times 63$ and corrected for random events, the attenuation of annihilation radiation, deadtime, scanner normalization, and scatter radiation. The reconstructed time series PET data were realigned using SPM8 (www.fil.ion.ucl.ac.uk/spm) to correct for subject motion during the course of the study. A denoising algorithm, highly constrained back-projection technique with backprojections to local ROIs, was then applied to the voxel-based time series [27]. The PET time series was coregistered into the T1-weighted MRI scan using mutual information.

The [C-11]PET data were then transformed into voxel-based parametric images representing [C-11]PiB binding, using the cerebellar cortex as a reference region of negligible binding [28]. Voxel-based parametric images using Logan graphical analysis were created as described by Lopresti et al. [28]. For the Logan graphical method [29], linear regression was applied to the transformed data using the 35- to 70-min (7 points) interval and a mean efflux constant of 0.149 min^{-1} . The resulting distribution volume ratio (DVR) images were inspected for quality. The three broad gray matter ROIs were used as masks to extract the bilateral mean value from the left and right hemispheres.

2.8. Statistics

For each ROI, a linear mixed model approach was used. The dependent measure was mean PiB signal extracted from one of the three ROIs, reflecting amyloid deposition. The fixed effect independent variable of interest was HOMA-IR by glycemic status. Fixed effect covariates included age at time of the scan, sex, FH status, *APOE* ϵ 4 status, BMI, and type 2 diabetes medication, and the main effects of glycemic status and HOMA-IR. Additional models were run that also incorporated education, DBP and SBP, or total cholesterol as covariates of secondary interest. The random effect of subject was modeled in all analyses. Although we included the main effects of glycemic status and HOMA-IR to test for their interaction, we only anticipated an interaction between HOMA-IR and glycemic status. Indeed, previous work has underscored the importance of examining HOMA-IR among participants with normoglycemia or hyperglycemia [13]. Holm-Bonferroni correction [30] was used to control type 1 error for the three ROI comparisons. This is a closed test procedure and maintains a family-wise alpha of 0.05 by getting unadjusted *P*-values of .017, .025, and .05 among the three null hypotheses tested. If the HOMA-IR by glycemic status interaction was

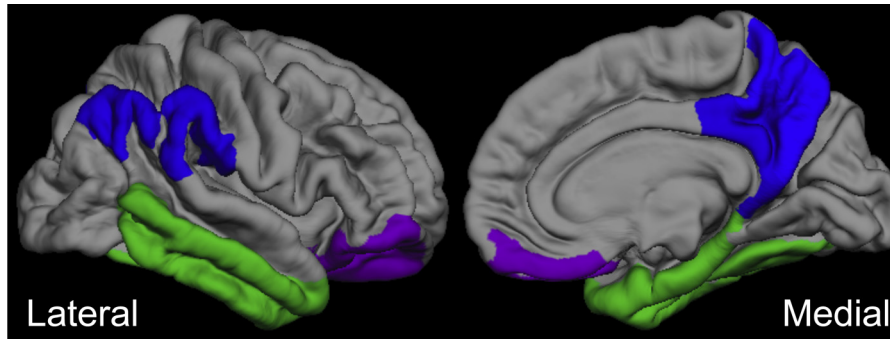


Fig. 1. Neural regions of interest (ROIs). Amyloid binding was broadly assessed in three bilateral ROIs: (1) a ventral frontal area in frontal lobe (“frontal ROI”); (2) an inferior and medial temporal area in temporal lobe (“temporal ROI”); and (3) a posterior medial parietal area in parietal lobe (“parietal ROI”).

significant, normoglycemia and hyperglycemia groups were separately tested with the same mixed model structure and covariates as above. HOMA-IR was the independent variable of interest in these post hoc analyses.

A logarithmic transformation was used to normalize HOMA-IR, which originally had positive skew (3.436). Nonparametric Mann-Whitney U tests were used to compare demographic characteristics between participants classified as PiB positive (PiB+) or PiB negative (PiB-), as described in the following section. Finally, to confirm that participants with high values did not bias HOMA-IR and PiB associations, a separate set of nonparametric analyses were conducted. Specifically, ROI values were first covariate adjusted using the same covariates as above, followed by Spearman correlations for each glycemic group. All analyses were conducted using SPSS 21.0 (Chicago, IL).

3. Results

3.1. Demographics and PiB deposition characteristics

Sample characteristics are listed in Table 1. We have previously classified and reported on WRAP participants that appear to be PiB+, PiB intermediate, and PiB-, and corresponding neural and cognitive features [18]. Based on a mean DVR of 1.1 or higher over any of the three broad ROIs in this preclinical, middle-aged cohort, 18 participants were classified as PiB+ compared with 168 PiB- participants. Based on the Mann-Whitney U statistic, PiB+ corresponded to significantly higher mean BMI [32.4 vs. 27.7, $U(184) = 932$, $Z = 2.670$, $P = .008$], glucose [114.1 vs. 93.0, $U(184) = 196$, $Z = 6.067$, $P < .001$], insulin [19.6 vs. 8.5, $U(184) = 779.5$, $Z = 3.390$, $P = .001$], and HOMA-IR [4.04 vs. 1.65, $U(184) = 645.5$, $Z = 3.992$, $P < .001$]. PiB+ participants were older [63.6 vs. 60.0 years, $U(184) = 961.5$, $Z = 2.54$, $P = .011$] but not more likely to have been FH+ versus FH- [$U(184) = 1431$, $Z = 0.477$, $P = .633$], APOE $\epsilon 4$ versus non-APOE $\epsilon 4$ [$U(184) = 1236$, $Z = 1.507$, $P = .132$], or have a different sex ratio [$U(184) = 1467$, $Z = 0.260$, $P = .795$]. This pattern of results remained identical when using t-tests (data not shown).

3.2. IR, hyperglycemia, and amyloid deposition in ROIs

Fig. 2 depicts raw PiB uptake images for illustration purposes. Additional models incorporating education, DBP and SBP, or total cholesterol showed nearly identical results (data not shown). For the frontal ROI, a significant HOMA-IR \times glycemic status interaction was found [$F(1,186) = 10.580$, $P < .001$], whereas the main effects were nonsignificant for HOMA-IR [$F(1,186) = 0.131$, $P = .718$] and glycemic status [$F(1,186) = 3.031$, $P = .084$]. The post-hoc mixed model for each glycemic group indicated that the normoglycemia group [$F(1,135) = 5.429$, $P = .021$], but not hyperglycemia group [$F(1,51) = 2.532$, $P = .118$], showed a significant, modest relationship between higher HOMA-IR and PiB uptake of $R^2 = .071$ (Fig. 3). A similar HOMA-IR \times glycemic status interaction was found for the temporal ROI [$F(1,186) = 6.109$, $P = .014$]. Post-hoc testing indicated that the normoglycemia group had a small but significant association [$F(1,135) = 4.751$, $P = .031$] between higher HOMA-IR and higher PiB uptake ($R^2 = .036$), whereas the association was nonsignificant for the hyperglycemia group [$F(1,51) = 1.389$, $P = .244$]. Although the HOMA-IR \times glycemic status interaction was significant for the parietal ROI [$F(1,186) = 5.056$, $P = .026$], neither the normoglycemia [$F(1,135) = 2.697$, $P = .103$] or hyperglycemia [$F(1,51) = 2.599$, $P = .113$] groups showed a significant HOMA-IR main effect during post-hoc testing. In a set of follow-up analyses, covariate-adjusted Spearman correlations between HOMA-IR and PiB in the three ROIs were conducted for the normoglycemia and hyperglycemia groups. We confirmed that the normoglycemia group showed modest associations between higher HOMA-IR and higher PiB in the frontal [$r = .195$, $P = .012$] and temporal [$r = .150$, $P = .020$] ROIs, but not the parietal ROI [$r = .090$, $P = .149$]. The hyperglycemia group showed no significant associations.

3.3. IR, hyperglycemia, and amyloid deposition in sub-ROIs

On an exploratory basis without type 1 error correction, we also investigated bilateral sub-ROIs depicted in Supplementary Fig. 1 that composed the three broad ROIs.

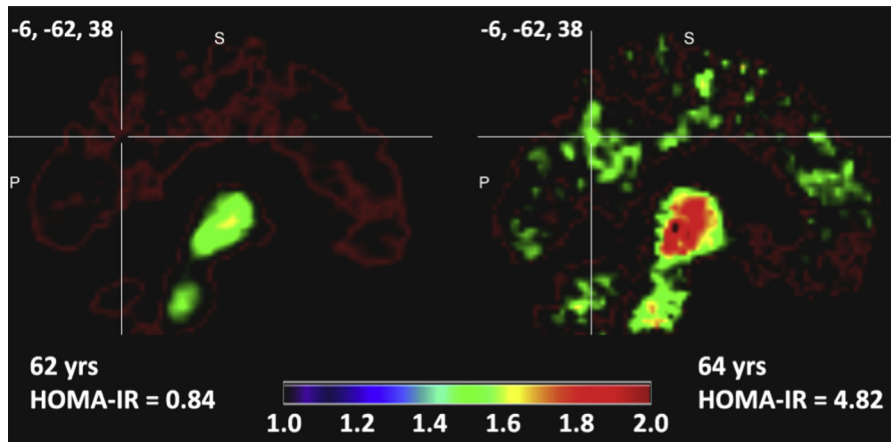


Fig. 2. Pittsburgh compound B (PiB) images and insulin resistance. Amyloid uptake images in age- and sex-matched representative participants, who varied by the homeostatic model assessment of insulin resistance (HOMA-IR). Two representative sagittal PiB images are shown for a participant with low IR (HOMA-IR <2) or high IR (HOMA-IR \geq 2). The color bar depicts the PiB distribution volume ratio (DVR), a quantitative index of PiB uptake.

Specifically, among 17 sub-ROIs, we tested the relationship between higher HOMA-IR and higher PiB in the normoglycemia and hyperglycemia groups. The hyperglycemia group showed no associations (data not shown). For the normoglycemia group, [Supplementary Table 1](#) indicates that the frontal ROI result may be explained by gyrus rectus. For the temporal ROI, significant subregions included inferior temporal gyrus and sulcus, and medial temporal lobe, where HOMA-IR explained 14.7% of the variance in inferior temporal gyrus. For the parietal ROI, no sub-ROI was statistically significant. We emphasize that these exploratory analyses should be viewed with caution, given the lack of error correction.

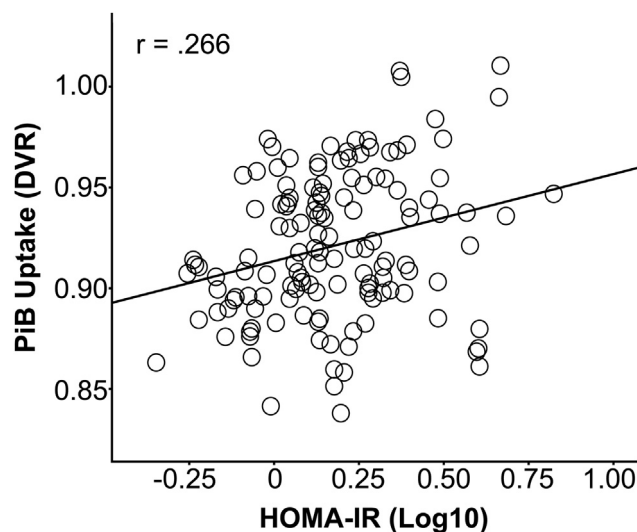


Fig. 3. Insulin resistance and frontal amyloid deposition. The association between higher homeostatic model assessment of insulin resistance (HOMA-IR) and higher a Pittsburgh compound B (PiB) frontal distribution volume ratio (DVR) in participants with normal glucose values. DVR values were adjusted by the following covariates: age, sex, apolipoprotein ϵ 4 status, family history of Alzheimer's disease (AD), taking type 2 diabetes medication, body mass index (BMI), and the main effects of HOMA-IR and glycemic status.

4. Discussion

The aim of this study was to determine the association of IR with glycemic status on PiB uptake in cognitively healthy, late-middle aged adults. This is the first study to illustrate an association between higher IR and an in vivo index of amyloid burden. This association was found only in participants without elevated glucose values, which we briefly discuss later. Although this relationship was modest for the broad ROIs, it is compelling to consider that these associations were found in an asymptomatic cohort only beginning to show amyloid deposition, given that there is a wide variation in the presence and degree of amyloid aggregates present even in aged adults without AD [31]. A similar amyloid pattern is seen in sporadic late onset AD [9]. IR has been linked with amyloidosis in both humans and animals [3,4,9], although others have found no relationship between IR and amyloid scans or histopathology [32]. Given that neural amyloidosis is one of the first salient features in preclinical AD [23], it may be of clinical relevance to test whether interventions that reduce IR may also reduce amyloid deposition and other aspects of disease pathogenesis in similar cohorts. However, one cannot infer causality or directionality about IR and amyloid burden from this study.

It should be cautioned that one should not extrapolate results from middle-aged participants without clinical impairment to MCI and AD or cognitively normal, aged participants. Indeed, it is noteworthy to mention that these results differ from Thambisetty et al. [32], who recently found that longitudinal insulin resistance derived from oral glucose tolerance tests did not predict PiB uptake or amyloid at autopsy in aged subjects. The PiB imaging component of their study had a comparatively smaller sample size than ours and did not covary typical AD risk factors. Furthermore, different insulin kits were used to analyze values over the course of the study, which might cause significant variation. Given that baseline HOMA-IR may only predict AD conversion out to 3 years [7], longitudinal HOMA-IR may also be less

important than HOMA-IR collected near scan time. Finally, Talbot et al. [8] found post-mortem that central IR increased from cognitively normal to AD participants, and was related to higher amyloid plaque load.

It has often been speculated that IR induces atrophy in part through amyloid neurotoxicity [33] and decreased glucose uptake [34], the latter of which can induce protein glycation and subsequent reactive oxygen species production. Tau aggregation and hyperphosphorylation may be mechanisms to consider, although tau pathology is hypothesized to occur later in the disease process [23]. IR also dysregulates vasodilation and damages microvascular architecture [35,36], which can cause microangiopathy. These events can precede type 2 diabetes onset [37,38]. If IR influences amyloid aggregation, it may only begin to affect brain volume later in life or during early AD, although again it is not appropriate to infer from the study that IR will predict amyloid deposition in AD.

Our primary analysis did not show a statistical effect among participants with hyperglycemia. These results may be due to the limited range of hyperglycemia in our sample, particularly the relatively few participants with type 2 diabetes. Hyperglycemia may also impact amyloid burden independent of IR. Given that type 2 diabetes increases AD risk [7], larger studies of amyloid binding in patients with frank diabetes, both treated and untreated, will be needed to further examine these associations.

Several limitations should be discussed. On average, the DVRs for [C11]PiB were low. However, similarly low DVR and mean cortical binding potential have been found in studies focused on a slightly older middle-aged cohort [39] or that in part examined middle-aged participants [40]. By extension, it was not feasible to examine PiB deposition in control regions unlikely to be affected by IR, because there is not a high enough DVR signal to be considered reliable in this healthy, middle-aged cohort. Although additional areas of interest could have been chosen for our analysis, we chose a small number of broad ROIs in which early amyloidosis or AD pathology is found, primarily to reduce and control type 1 error. The exploratory analysis of sub-ROIs within these broad ROIs especially warrants caution, as regional analyses were done without type 1 error correction. The associations between HOMA-IR and PiB DVR in broad ROIs were modest. However, Reiman et al. [39] found in several ROIs similar to ours that heterozygous or homozygous $\epsilon 4$ carriers had significant but similarly modest increases in PiB DVR, although they also found larger increases in other ROIs. It should again be noted that causal inferences cannot be drawn based on our study. Finally, because not all cognitively normal participants who show amyloid deposition will develop AD, we reiterate that it is inappropriate to infer that higher HOMA-IR is a risk factor for amyloid deposition in MCI and AD patients. In conclusion, cognitively normal middle-aged participants with high HOMA-IR had modestly higher amyloid binding in several regions impacted by early AD. IR may be an important biomarker for early amyloid deposition in middle-aged participants at higher risk for AD.

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Supplementary data

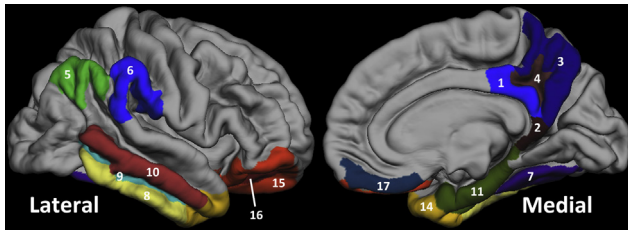
Supplementary data related to this article can be found at <http://dx.doi.org/10.1016/j.jalz.2014.03.011>.

RESEARCH IN CONTEXT

1. Systematic review: We searched for articles in PubMed using the following keywords: insulin resistance; amyloid; PiB; Pittsburgh compound B; $A\beta_{1-42}$; positron emission tomography; type 2 diabetes; metabolic syndrome; and Alzheimer's disease. We examined in vivo and ex vivo work in rodents and humans, to determine to what degree insulin resistance predicts amyloidosis and may serve as a biomarker for amyloid accumulation in tissue.
2. Interpretation: This is the first human study to demonstrate that insulin resistance (IR) is associated with amyloid deposition in brain regions affected by Alzheimer's disease (AD). These associations were found in late middle-aged participants only beginning to show amyloidosis, and the pattern reflects early AD progression.
3. Future directions: To confirm and expand on our work, it will be important to further examine IR and amyloid deposition in cognitively healthy and impaired older adults. Intervention studies are also needed to test the protective effect of IR reduction on AD prevention.

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Supplementary Fig. 1. Sub-regions of interest (sub-ROIs). Amyloid binding in the following FreeSurfer areas was used to initially construct the three broad ROIs of interest, as well as for use in exploratory analyses looking at homeostatic model assessment of insulin resistance (HOMA-IR) and bilateral Pittsburgh compound B (PiB) uptake in the normoglycemia group. Parietal lobe: posterior cingulate gyrus (1); posterior cingulate isthmus (2); precuneus (3); subparietal sulcus (4); angular gyrus (5); supramarginal gyrus (6). Temporal lobe: fusiform gyrus (7); inferior temporal gyrus (8); inferior temporal sulcus (9); middle temporal gyrus (10); parahippocampal gyrus (11); amygdala and hippocampus (12 and 13, not shown); temporal pole (14). Frontal lobe: orbital gyrus (15); orbital sulcus (16); gyrus rectus (17).

Supplementary Table 1
IR and bilateral PiB sub-ROI associations for participants with normoglycemia (N = 136)

Brain region	Adjusted R ²
Dorsal PCC	
Ventral PCC	
Precuneus	
Angular gyrus	0.014 [#]
Subparietal sulcus	0.035 [#]
Supramarginal gyrus	
Fusiform gyrus	
Inferior temporal gyrus	0.147**
Inferior temporal sulcus	0.064**
Middle temporal gyrus	0.058*
Amygdala	
Hippocampus	
Parahippocampal gyrus	
Temporal pole	
Orbital gyrus	
Orbital sulcus	0.018 [#]
Gyrus rectus	0.104*

Abbreviations: IR, insulin resistance; PiB, Pittsburgh compound B; PCC, Posterior Cingulate Cortex; ROI, region of interest.

NOTE. The adjusted R² reflects the proportion of variance explained in the sub-ROI by homeostatic model assessment of insulin resistance (HOMA-IR). For example, 0.147 reflects that 14.7% of the variance in inferior temporal gyrus is attributable to HOMA-IR.

[#]*P* < .10; **P* < .05; ***P* < .01.